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Q1 Co-activation Probability Estimation (CoPE): An approach for modeling 2 functional co-activation architecture based on neuroimaging coordinates

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A B S T R A C T

Recent progress in functional neuroimaging has prompted studies of brain activation during various cognitive tasks. 22
Coordinate-based meta-analysis has been utilized to discover the brain regions that are consistently activated across 23
experiments. However, within-experiment co-activation relationships, which can reflect the underlying functional 24
relationships between different brain regions, have not been widely studied. In particular, voxel-wise co-activation, 25
which may be able to provide a detailed configuration of the co-activation network, still needs to be modeled. To 26
estimate the voxel-wise co-activation pattern and deduce the co-activation network, a Co-activation Probability Es- 27
timation (CoPE) method was proposed to model within-experiment activations for the purpose of defining the co- 28
activations. A permutation test was adopted as a significance test. Moreover, the co-activations were automatically 29
separated into local and long-range ones, based on distance. The two types of co-activations describe distinct fea- 30
tures: the first reflects convergent activations; the second represents co-activations between different brain regions. 31
The validation of CoPE was based on five simulation tests and one real dataset derived from studies of working 32
memory. Both the simulated and the real data demonstrated that CoPE was not only able to find local convergence 33
but also significant long-range co-activation. In particular, CoPE was able to identify a 'core' co-activation network in 34
the working memory dataset. As a data-driven method, the CoPE method can be used to mine underlying co- 35
activation relationships across experiments in future studies. 36

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42 Introduction

Over the past two decades, researchers have used neuroimaging to 43
study the functional and structural aspects of the brain, leading to the 44
generation, analysis, and publication of large amounts of data. Conse- 45
quently, large scale accessible databases, such as BrainMap (Fox & 46
Lancaster, 2002; Laird et al., 2005) and NeuroSynth (Yarkoni et al., 47
2011), which compile published neuroimaging results, have arisen as re- 48
positories for the various types of information including peak coordinates 49
obtained from neuroimaging studies. The use of functional magnetic res- 50
onance imaging (fMRI) and diffusion tensor imaging (DTI) has helped to 51
generate great interest in investigating the functional and structural 52

connectivity of the human brain. Although the number of connectivity- 53
based neuroimaging studies that employed tasks is fewer than the ones 54
that studied the resting state, the growing number of these task-based 55
studies provides a significant opportunity to expand our knowledge of 56
task-dependent functional connectivity in order to identify "emergent 57
properties", i.e., to discover classes of observations not reported in the 58
source publications (Fox & Friston, 2012; Laird et al., 2013). 59

In the first such study, Toro et al. (2008) used chi-square calculations 60
to investigate the relationship between the task-dependent co- 61
activation pattern and canonical functional brain networks, such as the 62
default mode network. As meta-analytic techniques have improved, 63
the evolving family of coordinate-based meta-analysis (CBMA) 64
methods has offered data-driven techniques to quantitatively synthe- 65
size the consistent functional activation. In general, CBMA is based on 66
three-dimensional coordinates in MNI (Evans et al., 1992) or Talairach 67
(Talairach & Tournoux, 1988) standard reference space. Common 68
CBMA methods are activation likelihood estimation (ALE; (Eickhoff 69
et al., 2012; Eickhoff et al., 2009; Turkeltaub et al., 2002)) and related 70

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techniques, such as (multilevel) kernel density analysis (KDA and MKDA; (Wager et al., 2004; Wager et al., 2007)). A new meta-analytic technique based on ALE, meta-analytic connectivity modeling (MACM), is able to investigate task-dependent connectivity (Eickhoff et al., 2010; Laird et al., 2009; Robinson et al., 2010). In principle, MACM is a seed-based method which estimates the activation-dependent connectivity for a user-defined region of interest. Another method, independent component analysis (ICA), can be used to mine the architecture of task-dependent networks in the BrainMap database. The task-dependent networks also match the pattern from resting state fMRI data from healthy subjects (Ray et al., 2013; Smith et al., 2009). Other researchers (Poldrack et al., 2012) used a topical mapping method to extract the task-dependent networks from the NeuroSynth database. The networks they obtained were also similar to the networks obtained using resting state data (Poldrack et al., 2012).

These previously-mentioned methods could deduce significantly convergent activated regions and interpret them as network distributions. However, these methods may have disadvantages when configuring a detailed connectivity pattern between any two activated brain regions or voxels. Specifically, the MACM method, which is based on defining a region of interest, i.e., a seed-based method, may not be feasible if the integration or co-activation between any two seeds is taken into account because the co-activations will need to be calculated one by one. The other method, i.e., the ICA-based method, can identify the architecture of a task-dependent co-activation network, but the configuration of the network may not be detected, i.e., all of the above-threshold brain regions identified using the ICA-based method may be considered as consistently co-active. For example, if the ICA-based method found that brain regions A, B, and C were above the threshold, a situation could quite possibly exist in which A and B are co-activated, and B and C are also co-activated, but A and C are not co-activated. In this situation, the two activated brain regions did not have the same connectivity or functional co-activation relationships. On the other hand, the ICA-based method necessitates using a large number of experiments to satisfy the sample size demanded by the ICA method. For example, a specific cognitive dataset, such as one using experiments about working memory, might not have a sufficient number of experiments, causing sample size to be a problem.

In order to determine the voxel-wise configuration of co-activation networks, we proposed a method we called CoPE, which modeled the activation around peak foci by making a map of the Gaussian distribution around each focus within each experiment. Using co-occurrence within the same experiment as the criterion, CoPE defined the voxel-wise co-activations across the experiments. Then, a permutation test was introduced into CoPE as a significance test. Further, CoPE could separate the co-activation patterns into either local or long-range, based on a well-defined distance. On one hand, local co-activation reflects local convergence in a manner similar to that of the ALE method. Local co-activation is mainly generated from the model. On the other hand, long-range co-activation reflects consistent within-experiment co-activation between distant regions. Mining the interaction effects of the underlying task-dependent network is of particular interest. To evaluate the CoPE method, we employed five simulation datasets and a real working memory dataset to test whether the method could mine the architecture and the configuration, i.e., the co-activation relationship, of the co-activation network, especially long-range patterns from large datasets.

Materials and methods

In practice, few neuroimaging experiments can report more than a dozen foci for a given contrast, i.e., the activation foci are sparsely distributed around the brain. So, CoPE only takes co-activations into account, i.e., non-occurrences between two foci are not modeled. There are three steps in the CoPE method: The first is to map the peak foci onto activation maps after calculating the Gaussian distribution around

each focus within each experiment. The second step is to obtain the weight of the co-activation between any two voxels using the individual activation map from step 1. The third step is to perform a permutation test to determine the significance of the co-activation. Fig. 1 gives an overview of the CoPE method.

Mapping the peak foci

Like the ALE method, CoPE uses a three-dimensional Gaussian distribution to model activation around individual coordinates. So, let $C_i = \{c_1^i \dots c_{n_i}^i\}$ be the reported foci in the i th experiment, where n_i is the number of foci in the i th experiment. Let $G(c_j^i, \Sigma_i)$ represent a three-dimensional Gaussian distribution centered at coordinate c_j^i , where Σ_i is the three-dimensional diagonal covariance matrix. The elements on the diagonal are the same and can be defined according to the empirical estimates provided by Eickhoff et al. (2009). The empirical estimate is based on the inter-subject and inter-template variability. In order to assess the modeled activation distribution in one experiment, the Parzen-window density estimation method (Parzen, 1962; Rosenblatt, 1956) was adopted to model the activation map. In this way, let AM_i be the activation map for the i th experiment, where AM_i can be formalized as

$$AM_i(v) = \frac{1}{n_i} \sum_{j=1}^{n_i} G(v; c_j^i, \Sigma_i)$$

with v denoting a voxel. This process was repeated to form an activation map for each experiment.

Modeling the voxel-wise co-activations

The co-activation relationship, i.e., the activated coordinates reported in a single experiment, is the key idea behind CoPE. In theory, the definition of co-activation between two voxels could be the product of the individual probabilities of the activations from the activation map, i.e., the estimated probability density function (pdf), for the experiment. However, accuracy will be an issue if the probability is directly generated from the estimated pdf. Because the voxel resolution used in CoPE is $2 \times 2 \times 2$ mm, the estimated pdf will contain a lot of small values for a large number of voxels, causing problems with accuracy if these are multiplied by each other. More importantly, the significance test in next step will need a much higher accuracy to distinguish the difference between co-activation weights, if we define the co-activation as the direct product of probabilities from the estimated pdf. In addition, each experiment was considered as independent, and, the experiments need to be comparable. So, a normalization procedure was adopted to increase the comparability between experiments. In detail, let $V = \{v_1, \dots, v_{n_v}\}$ be the voxel set, where n_v is the number of voxels. So, the normalized activation weight for the voxel x in the i th experiments can be defined as

$$P_i(v_x) = \frac{AM_i(v_x)}{AM_i(v_x) + \max(AM_i(v_x))}$$

where $P_i(v_x)$ is the normalized weight for the activation at voxel x in the i th experiment. The $\max(AM_i(v_x))$ is the maximum weight for the activation in the i th experiment. The nonlinear form of normalization is based on the consideration which is to emphasize the activation weight close to the informative part (the part of high activation weight) in a given experiment. After converting the probability density into the normalized activation weight, the weight of the co-activation between any two voxels across experiments can be defined as

$$CoW_{x,y} = \sum_{i=1}^{n_{exp}} P_i(v_x) * P_i(v_y)$$

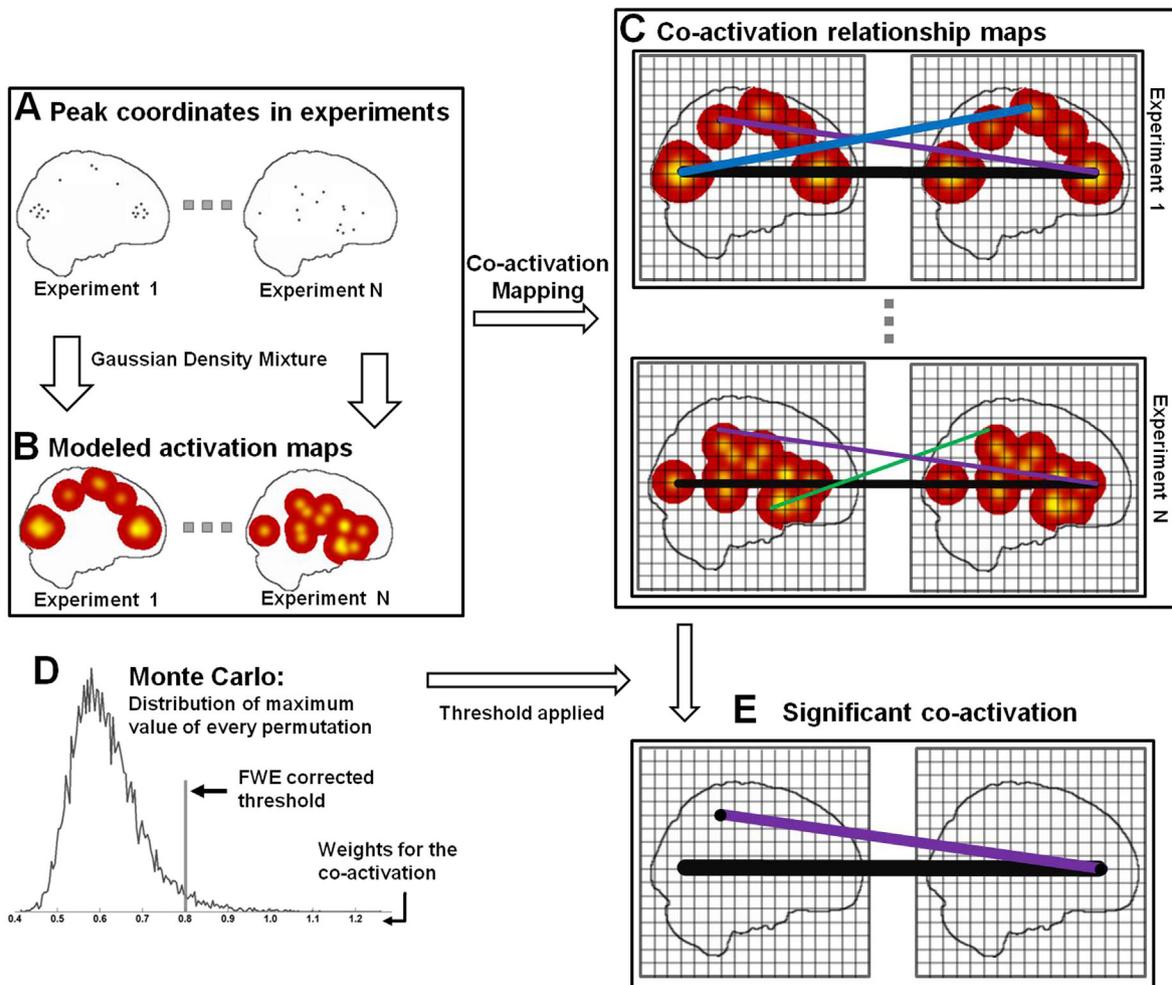


Fig. 1. Schematic representation of the procedures for CoPE. (A) Identifying the peak coordinates from N experiments. (B) Treating each peak coordinate in each experiment separately as the center of a 3D Gaussian probability distribution and combining the distribution functions to provide a specific density function for each experiment. The density in each voxel was used to model the activation in each experiment. (C) Defining the voxel-wise co-activation relationships. In each experiment, the lines (for example, the black line) represent co-activation between the voxels at each end. (D) Deriving the null-distribution which can reflect the random spatial co-activation across experiments. The peak coordinates in each experiment were randomly permuted, and the maximum value of the co-activation from each permutation was used to create a random co-activation map with which to compare the actual co-activation map. (E) Deriving the voxel-based significant co-activation relationships. All the co-activation relationship maps were pooled, and the threshold for the pooled weight of each line was used to identify the lines that represented significant co-activation (for example, the black and the purple ones).

185 where $\text{CoW}_{x,y}$ represents the co-activation weight between voxels x and y across experiments. n_{exp} is the number of the experiments. The
 186 necessity of the normalization is illustrated by the calculation of
 187 $\text{CoW}_{x,y}$, which guarantees the accuracy of the calculation. Obviously,
 188 co-activations with high weights correspond to a high probability of
 189 consistency among the experiments.

190 Inference based on the permutation test

191 Due to the nonlinear calculation of $\text{CoW}_{x,y}$, a parametric inference
 192 based on the Gaussian random field was not feasible (Eickhoff et al.,
 193 2012). In addition, the false discovery rate (FDR) is not the optimal
 194 approach for making inferences about the topological features derived
 195 from ALE-like meta-analysis methods (Eickhoff et al., 2012). So, the
 196 nonparametric family-wise error rate (FWE) correction for multiple
 197 comparisons was used. More specifically, the nonparametric FWE
 198 correction was based on a Monte-Carlo analysis, i.e., the reported coordi-
 199 nates in each experiment are randomly redistributed throughout the
 200 gray matter of the brain in each permutation. The gray matter mask
 201 was based on ICBM (The International Consortium for Brain Mapping)
 202 gray matter maps with a probability above 10% (Evans et al., 1994). In
 203 each permutation, the number of coordinates and the number of

204 subjects in each experiment were kept unchanged. The co-activation
 205 weight between voxels, i.e., $\text{CoW}_{x,y}$, was calculated in each permuta-
 206 tion. The maximum value of $\text{CoW}_{x,y}$ was preserved for subsequent infer-
 207 ence. To this end, the distribution of the maximum co-activation
 208 weight was used for the FWE correction (Nichols & Hayasaka, 2003).
 209 In fact, if the distribution of the maximum redistributed co-activation
 210 weight is calculated strictly as mentioned earlier, the time cost will be
 211 too high. For example, performing 5000 permutations on a dataset of
 212 about 180 experiments and about 3000 coordinates would take one to
 213 two days to calculate using a computer running at 2.4 GHz with 16 GB
 214 of memory. Here, we provided an alternative approach for estimating
 215 the compact upper bound of the maximum co-activation weight in
 216 each permutation. Replacing the maximum co-activation weight with
 217 the upper bound allowed us to save a great deal of calculation cost
 218 while providing a conservative estimate of the FWE correction. More
 219 precisely, the key idea behind the approach is based on the Cauchy-
 220 Schwarz inequality (Kadison, 1952; Steele, 2004), in which the calcula-
 221 tion of the co-activation weight satisfies

$$\text{CoW}_{x,y}^k = \sum_{i=1}^{n_{exp}} P_i(v_x, k) * P_i(v_y, k) \leq \sqrt{\sum_{i=1}^{n_{exp}} P_i(v_x, k)^2 \sum_{i=1}^{n_{exp}} P_i(v_y, k)^2} = \text{up-CoW}_{x,y}^k$$

223 where $CoW_{x,y}^k$ is the co-activation weight between any two voxels in the
 224 k th permutation. $P_i(v_x, k) > 0$ and $P_i(v_y, k) > 0$ are the normalized
 225 weights of the activations within the i th experiment at any voxel in
 226 the k th permutation. $up_CoW_{x,y}^k$ is the upper bound of $CoW_{x,y}^k$. After
 227 the conversion, the maximum value of the co-activation weight in
 each permutation is calculated by the simplified formula

$$CoW_{max}^k \leq \max(up_CoW_{x,y}^k)$$

229 where CoW_{max}^k represents the maximum co-activation weight in the k th
 permutation. The calculation of the maximum of $up_CoW_{x,y}^k$ is based on
 230 the descending sort of $\sum_{i=1}^{n_{exp}} P_i(v_x, k)^2$ across all voxels. After sorting, the
 231 product of the first two values in the descending order corresponds to
 232 the maximum of $up_CoW_{x,y}^k$.

233 Local convergence and long-range co-activation

234 In fact, the co-activations for each voxel fall into two types defined
 235 by distance: local convergence and long-range co-activation. In the
 236 case of local convergence, the co-activation weight between the peak
 237 coordinate and the local neighborhood directly around it should be
 238 high, because the coordinate is modeled by the activations that fit a
 239 Gaussian distribution. However, our particular interest was to mine
 240 the interaction effect of the underlying task-dependent network,
 241 which is represented by long-range co-activations. The distance used
 242 to distinguish the local and the long-range co-activation was defined as

$$D = 3\delta$$

244 where D is the distance (in mm) for distinguishing between local con-
 vergence and long-range co-activation, and, $\delta = \sqrt{\frac{7.3^2}{N_{subj}} + 3.6^2}$. N_{subj}

245 is the mean number of subjects across the experiments. δ is the empir-
 246 ical estimate of the standard deviation for the modeled Gaussian distri-
 247 bution (Eickhoff et al., 2009). Voxels that were 3δ away from the
 248 reported focus were considered to be distant, because the probability
 249 of their being physically near the focus was negligible. Consequently,
 250 co-occurrences beyond this range would not be likely to be driven by
 251 a local convergence of the foci but rather represent true co-activation.
 252 In order to measure the level of significant co-activation amount at
 253 each voxel, the weights of all the significant co-activations with that
 254 voxel were added together. The degree density map (DDM) was defined
 255 as a map of the summed weights for each voxel. An example of the calcu-
 256 lation of a DDM is provided in Supplemental Fig. 1. Further, each DDM
 257 was separated into two parts: local and long-range. Specifically, the
 258 local DDM was defined as the whole brain degree distribution restricted
 259 by distance D , i.e., only local convergence was considered. The long-
 260 range DDM referred to the whole brain co-activation distribution be-
 261 yond distance D , i.e., only long-range co-activations were considered.

262 Evaluation of the CoPE method

263 To evaluate the CoPE method, we analyzed several simulated
 264 datasets. In addition, we analyzed a real dataset about working memory
 265 to see if we could use the reported coordinates to determine the configu-
 266 ration of the task-dependent co-activation network. The ability of CoPE
 267 to find the convergent activation regions was validated by comparing
 268 the CoPE results with those found using ALE. The simulated datasets
 269 had two basic properties in common. First, the simulated peak foci in
 270 each experiment were randomly derived from a special Gaussian distri-
 271 bution centered at a designated center. In each experiment, the stan-
 272 dard deviation for the Gaussian distribution was calculated using the
 273 method in Eickhoff et al. (2009). Second, the number of subjects in

each experiment was randomly generated, with a range of 14 to 30
 274 participants. 275

Each of the five simulations for the CoPE method had some type of
 276 special property. Simulation 1 was designed to test whether CoPE
 277 could find the convergent activation region across a set of experiments.
 278 Convergent activation was a necessary condition for the co-activation
 279 analysis in the next step. In this case, an extreme situation in which
 280 only one peak focus was found in each experiment was considered. By
 281 using only one focus, we could ensure that there was no co-activation
 282 between reported foci. Any voxel-wise 'co-activation' came completely
 283 from the model. Although it only used the modeled co-activation, Sim-
 284 ulation 1 was expected to show whether the convergent region was
 285 similar to the activation results obtained using ALE. More specifically,
 286 the dataset consisted of 50 experiments, each of which included 1 re-
 287 ported coordinate that was randomly derived from the Gaussian distri-
 288 bution centered at this location: MNI: 0 8 64. 289

Simulation 2 was an expansion of Simulation 1 to test whether CoPE
 290 could detect not only multiple convergent activation regions but also
 291 the co-activation relationship across different regions. Specifically, we
 292 designed 50 experiments in each of which were two reported coordi-
 293 nates randomly derived from two individual Gaussian distributions cen-
 294 tered at two centers: Simulated point 1 (SP1, MNI: 0 8 64) and
 295 Simulated point 2 (SP2, MNI: 0–76 6). 296

Simulation 3 was a supplement to Simulation 2 to determine wheth-
 297 er CoPE could distinguish an absence of co-activation between two acti-
 298 vated regions. Specifically, we designed 100 experiments, 50 of which
 299 had one peak coordinate in each experiment randomly derived from
 300 the Gaussian distribution centered at Simulated point 1 (SP1, MNI: 0 8
 301 64) and the other 50 of which had one peak coordinate in each
 302 experiment with the Gaussian distribution centered at Simulated
 303 point 2 (SP2, MNI: 0–76 6). 304

The goal of Simulation 4 was to test whether CoPE would be able to
 305 detect both local convergence and long-range co-activation. Specifically,
 306 we designed three centers: Simulated point 1 (SP1, MNI: 0–74 8), Sim-
 307 ulated point 2 (SP2, MNI: 0 48 12) and Simulated point 3 (SP3, MNI: 0 0
 308 54). Once again, we designed 100 simulated experiments, 50 of which
 309 had one peak focus from the Gaussian distribution centered at SP3
 310 and the other 50 had two peak foci individually derived from the two
 311 Gaussian distribution centered at SP1 and SP2. Thus, in this simulation
 312 SP1 and SP2 were co-activated, but SP3 was only activated. 313

Simulation 5 investigated the effect of noise on CoPE. Specifically, we
 314 designed five centers: Simulated point 1 (SP1, MNI: –12 –16 8), Simu-
 315 lated point 2 (SP2, MNI: 12 –18 6), Simulated point 3 (SP3, MNI: –56
 316 –16 36), Simulated point 4 (SP4, MNI: 56 –16 36) and Simulated
 317 point 5 (SP5, MNI: 0 6 60) with five random noise levels: Level 1
 318 (noise coordinates to information coordinates: 10:1), Level 2 (noise co-
 319 ordinates to information coordinates: 3:1) and Level 3 (noise coordi-
 320 nates to information coordinates: 1:1). Two additional levels were also
 321 tested to test the extremes. One of these had no random noise and the
 322 other had an extreme noise level, in which the ratio of noise coordinates
 323 to informative coordinates was 100:1. In all, each simulation utilized 100
 324 experiments, 50 of which had two peak foci individually derived from
 325 the two Gaussian distributions centered at SP3 and SP4. The other 50 ex-
 326 periments utilized three peak foci derived separately from SP1, SP2 and
 327 SP5. The random noise called for by each noise level was added to each
 328 experiment so that it was uniformly distributed across the brain mask. 329

The real dataset was obtained from a recent coordinate-based meta-
 330 analysis on working memory (Rottschy et al., 2012). This dataset
 331 consisted of 189 experiments with 2662 activation foci. Differences in
 332 the reported coordinates were transformed from Talairach space to
 333 MNI space using the Lancaster transform (Lancaster et al., 2007). The
 334 dataset had been collected by hand from the BrainMap dataset and
 335 the PubMed literature (see more detail in Rottschy et al., 2012). 336

ALE and CoPE were applied to the simulation datasets and the work-
 337 ing memory dataset. ALE was performed by the GingerALE desktop ap-
 338 plication (<http://www.brainmap.org/ale>) using the approach provided
 339 339

340 in Eickhoff et al. (2012) and Eickhoff et al. (2009). The correction meth-
 341 od used in ALE was a cluster-level FWE correction. The cluster was
 342 formed using a voxel-level threshold of $p < 0.001$. In the CoPE method,
 343 a permutation test with 5000 permutations was used to control the
 344 FWE rate.

345 Results

346 Simulation datasets

347 Simulation 1 was used to discover whether CoPE could find the conver-
 348 gent activation region across the experiments. The DDM that re-
 349 vealed the modeled co-activation found by using CoPE was very
 350 similar to the activation map from ALE. The pattern of the convergent
 351 region obtained using CoPE corresponded to the pattern of the consis-
 352 tently activated region obtained using ALE (Fig. 2A). In addition, the
 353 modeled co-activation relationship that passed the FWE correction is
 354 shown in Fig. 2B. The modeled co-activation was dense around the sim-
 355 ulation point (MNI: 0 8 64).

356 Simulation 2 indicated that CoPE could find the co-activations be-
 357 tween different activation regions. Similar regions were detected by
 358 both ALE and CoPE (Fig. 3A). Fig. 3B presents the voxel-wise significant
 359 co-activation relationships. Consistent with the test design for Simula-
 360 tion 2, co-activation was found between the regions around SP1 and
 361 SP2.

362 As a supplement to Simulation 2, Simulation 3 presented a situation
 363 in which the two regions had no co-activations. The activation map
 364 from ALE was similar to the DDM from CoPE in Simulation 3 (Fig. 4A).
 365 Moreover, the absence of co-activation between the two regions was
 366 found by CoPE (Fig. 4B), i.e., there was no co-activation relationship be-
 367 tween the regions around SP1 or SP2.

368 Simulation 4 was designed to determine whether CoPE could distin-
 369 guish local convergence from long-range co-activation in the same
 370 dataset. Fig. 5A presents the distribution of the dense co-activation re-
 371 gions around the simulated points (SP1, SP2 and SP3). In the simulation,
 372 3δ was used to distinguish between local convergence and long-range
 373 co-activation. δ was calculated as described in the Materials and
 374 methods section. In the simulation dataset, \overline{N}_{subj} was 21.3, yielding a
 375 3δ of 11.7 mm. Using this criterion, the local DDM is presented in
 376 Fig. 5B, which shows similar distributions around the simulated points.
 377 In Fig. 5C, the long-range DDM showed that only the regions around SP1
 378 and SP2 possessed long-range co-activations, a finding which was con-
 379 sistent with the simulation design. The detailed voxel-wise co-
 380 activation relationship is presented in Fig. 5D. Meanwhile, this simula-
 381 tion showed no long-range co-activation between SP3 and the others
 382 (SP1 and SP2).

383 In Simulation 5, simulation datasets with different levels of random
 384 noise were used to evaluate the CoPE method. As expected, given the
 385 design of the simulation, co-activation occurred between the regions
 386 around SP3 and SP4. In addition, the regions around SP1, SP2 and SP5
 387 possessed co-activation relationships between any pair of the regions.
 388 CoPE was able to identify co-activation relationships consistent with
 389 the design at the different noise levels, although the extent of the co-
 390 activations was not precisely the same across the various noise levels.
 391 The DDM and the voxel-wise co-activation matrix for the noise-free
 392 dataset are presented in Fig. 6A. The co-activation relationship was con-
 393 sistent with the designed one (co-activations between SP1, SP2, and
 394 SP5; co-activation between SP3 and SP4). The co-activation relationship
 395 was preserved even with an increase in noise level (Fig. 6B–D). More-
 396 over, similarity in the distribution of the regions with dense co-
 397 activations was also preserved, although the extent of these regions
 398 was a little different from the result from the noise free dataset (DDM
 399 in Fig. 6A–D). In the extreme situation (noise: informative foci 100:1),
 400 although the co-activation was weaker, the regions corresponding to
 401 the design in Simulation 5 could still be found (Supplemental Fig. 2).
 402 In detail, little co-activation was found between the region around SP3
 403 and the region around SP4. Co-activation was found between the re-
 404 gions around SP1, SP2, and SP5. Only individual local convergence was
 405 found around SP1, SP2, and SP5 (Supplemental Fig. 2).

Working memory dataset

406 The working memory dataset was used to evaluate CoPE in a real ap-
 407 plication. The long-range co-activations mined from the dataset were
 408 particularly interesting in that they showed co-activation relationships
 409 between several core brain regions. In detail, the DDM and the local
 410 DDM were both similar in the distributions of the significant regions
 411 to those obtained using ALE (see Fig. 7A, B, and C). However, the long-
 412 range DDM differed from the ALE result when the co-activation was re-
 413 stricted by distance (>12.12 mm; calculated as 3δ based on a \overline{N}_{subj} of
 414 14.6). Although the ALE and the DDM (Fig. 7A & B, respectively)
 415 reflected different aspects of the dataset, they showed similar results.
 416 In the ALE result, the significant regions (Fig. 7A) included the bilateral
 417 inferior frontal gyrus (IFG; extending to the Brodmann area 44 (BA
 418 44)), the bilateral middle frontal gyrus (MFG), the supplementary
 419 motor area (SMA), the bilateral insula (Ins), the bilateral inferior parietal
 420 lobule (IPL), the bilateral superior parietal lobule (SPL), the left basal
 421 ganglia (BG), the bilateral ventral visual cortex, and lobule VI of the cer-
 422 ebellum. According to the DDM, the regions with a high density (Fig. 7B)
 423 were the bilateral IFG (extending to BA44), the bilateral MFG, the SMA,
 424 the bilateral Ins, the bilateral IPL, and the bilateral SPL. For the local
 425 DDM, the regions with dense local convergence (Fig. 7C) were 426

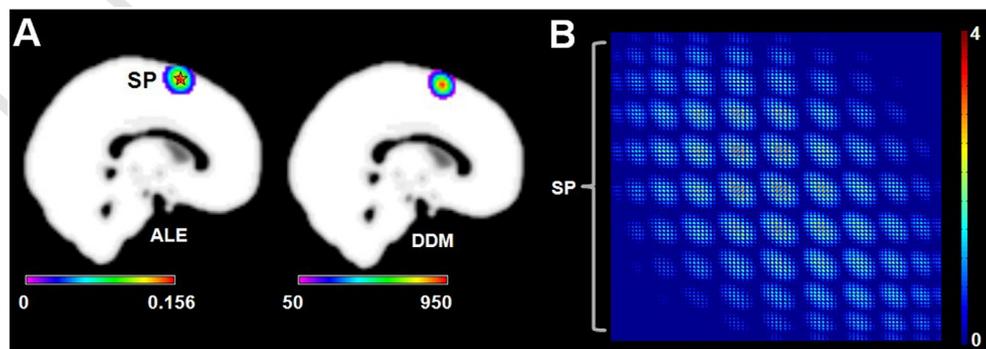


Fig. 2. Results of Simulation 1. (A) Left: the ALE results based on the simulation data. The pentagram represents the center (MNI: 0 8 64) of the simulation data. The result was corrected at $p < 0.01$ using a cluster-level FWE correction. Right: the degree density map (DDM) derived from the FWE-corrected voxel-wise co-activation matrix. (B) The significant voxel-wise co-activation matrix from CoPE. The threshold was $p < 0.01$ using an FWE correction. Each node of the matrix corresponds to a voxel which had a significant co-activation with other voxels. Each column lists all the significant co-activation relationships that a voxel had with other voxels.

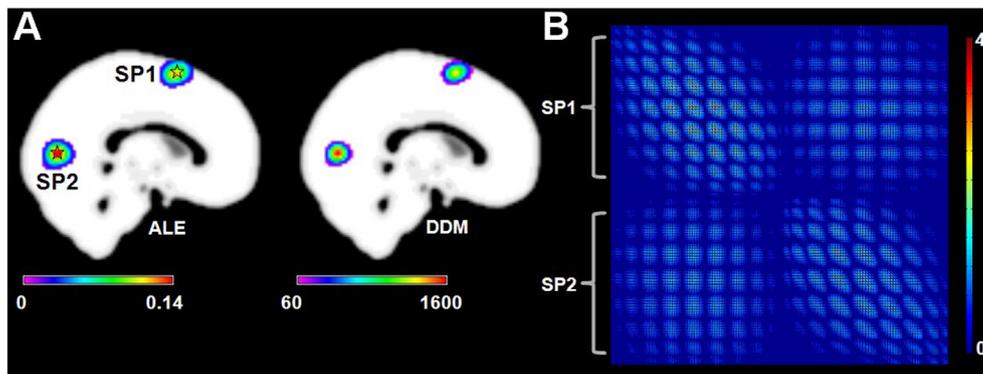


Fig. 3. Results of Simulation 2. (A) Left: the ALE results based on the simulation data ($p < 0.01$, corrected by a cluster-level FWE). The pentagrams represent the centers (MNI: 0 8 64; 0 – 76 6) of the simulation data. Right: the degree density map (DDM) derived from the FWE-corrected voxel-wise co-activation matrix. (B) The significant voxel-wise co-activation matrix from CoPE. The threshold was $p < 0.01$ using an FWE correction. Each node of the matrix corresponded to a voxel which had a significant co-activation with other voxels. Each column lists all the significant co-activation relationships that a voxel had with other voxels.

distributed in the bilateral IFG (extending to BA 44), the bilateral MFG, the SMA, the bilateral Ins, the bilateral IPL, and the bilateral SPL. For the long-range DDM, the main co-activated regions (Fig. 7D) were located in the left IFG (extending to BA44), the SMA, the bilateral Ins, and the left inferior parietal lobule (IPL). Moreover, no significant long range co-activation was found around the right IPG although this had showed up in the results from the ALE and the local DDM (see Fig. 7A, C, and D). The activation extent was smaller in the long-range DDM compared with the local DDM (see Fig. 7C and D). Because long-range co-activation was the main focus of this study, the long-range co-activation was analyzed. In detail, five spatially contiguous clusters were derived from the long-range DDM to define the regions of interest (ROI). We used the criterion of whether a voxel was one of the 26 nearest neighbors to another voxel to determine whether they were in the same ROI or a separate one. The five clusters corresponded to the regions in Fig. 7D and are shown in 3D in Fig. 8B. The voxel-wise long-range co-activation between the clusters is presented in Fig. 8A, which shows the detailed configuration of the co-activation relationship based on the working-memory dataset. In Fig. 8B, the co-activation relationship between any two clusters is shown in 3D. Long-range co-activations were detected between the bilateral Ins, SMA, and left IPL. Between the left BA 44 and the SMA, there was significant co-activation. The long-range core co-activations for the working-memory dataset appeared to form a left-lateralized network, with the exception of the inclusion of the right Ins.

Discussion

In this current study, we proposed a new approach, which we named CoPE, to infer voxel-wise task-dependent co-activation networks based on coordinates reported in neuroimaging experiments. The significance of the co-activations was identified using a permutation test. The CoPE method was able to distinguish between different types of co-activations, especially between long-range ones and local convergence.

The sparseness of peak foci

CoPE is restricted in modeling the co-activation across experiments. Theoretically, the co-activation and non-co-activation should be equally considered. However, the current experiments usually report only a few foci. It is difficult to distinguish whether the non-reported foci are informative or not. For example, there were 2662 peak foci in the current working memory dataset, but most of these foci (2559) were only reported once. So, we only took the reported foci into consideration. After using the Parzen window density estimation method, we modeled the activation in each experiment. In theory, there was no absolute zero at any voxel no matter how small the activation weight was. Although the approach restricted in activation foci was suboptimal, it obtained more confidence given the special property of the peak foci.

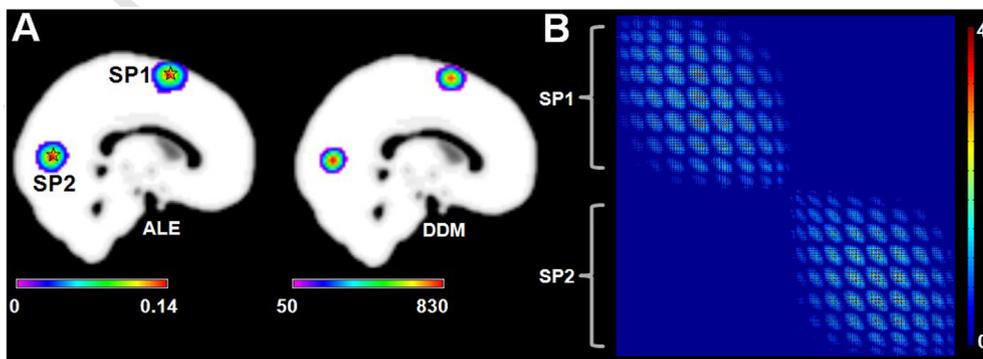


Fig. 4. Results of Simulation 3. (A) Left: the ALE results based on the simulation data. The pentagrams represent the centers (MNI: 0 8 64; 0 – 76 6) of the simulation data. The result was corrected at $p < 0.01$ using a cluster-level FWE correction. Right: the degree density map (DDM) derived from the FWE-corrected voxel-wise co-activation matrix. (B) The significant voxel-wise co-activation matrix from CoPE. The threshold was $p < 0.01$ using an FWE correction. Each node of the matrix corresponded to a voxel which had a significant co-activation with other voxels. Each column lists all the significant co-activation relationships that a voxel had with other voxels.

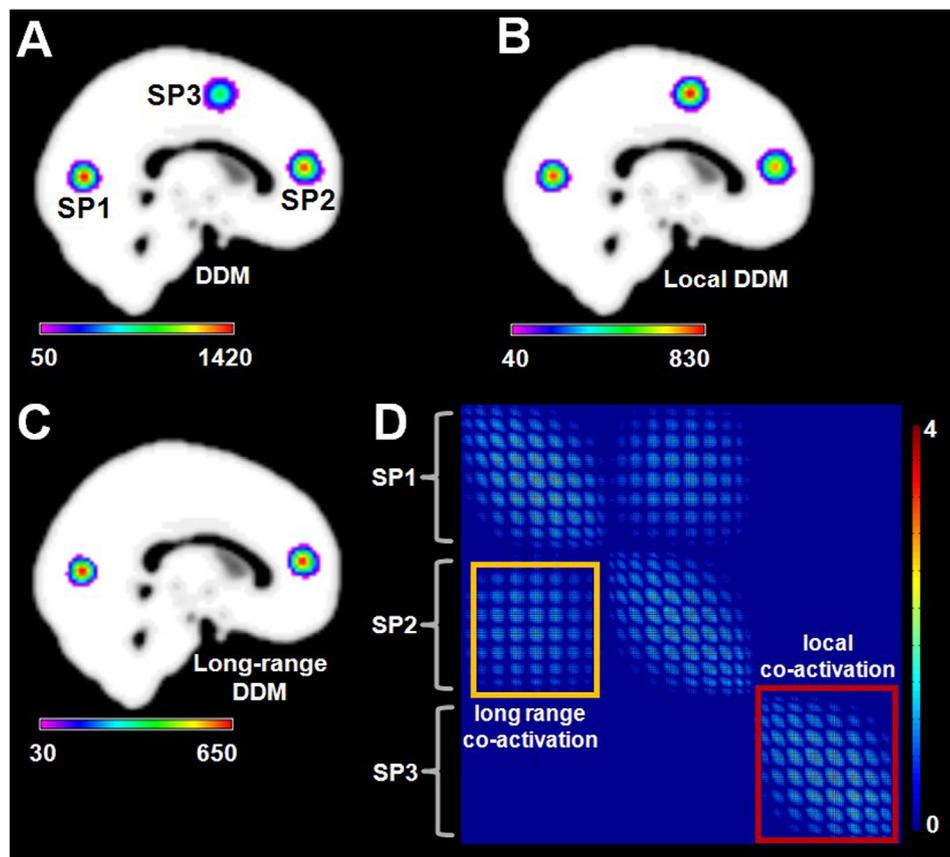


Fig. 5. Results of Simulation 4. The co-activation relationship was designed so that the only co-activation relationship was between SP1 and SP2. (A) The degree density map (DDM) derived from the FWE-corrected voxel-wise co-activation matrix. The statistical significance of the co-activation was derived based on an FWE at $p < 0.01$. The centers of this simulation were at (MNI: 0 - 74 8; 0 48 12; 0 0 54). (B) The local DDM obtained using the CoPE method. The co-activations were separated into local and long-range based on a distance of 11.7 mm. (C) The long-range DDM (long DDM) obtained using the CoPE method. (D) The significant voxel-wise co-activation matrix from CoPE. The threshold was $p < 0.01$ using an FWE correction. Each node of the matrix corresponds to a voxel which had a significant co-activation with other voxels. Each column lists all the significant co-activation relationships that a voxel had with other voxels.

473 Within-experiments effect

474 The within-experiments effect refers to the effect of finding multiple
 475 foci that are close together and/or of finding many foci in a single exper-
 476 iment. If a study focused on each individual coordinate, i.e., treated each
 477 coordinate as independent (a fixed effect), the study could easily be bi-
 478 ased by experiments with a greater number of activation coordinates.
 479 So, treating individual experiments as independent (a random effect)
 480 would help to avoid the within-experiments effect. For the ALE method,
 481 Turkeltaub et al. (2012) proposed to set the weight of a voxel according
 482 to the nearest reported coordinate in an individual experiment in order
 483 to weaken the within-experiments effect. For CoPE, we considered the
 484 within-experiments effect differently. Specifically, CoPE used the Parzen
 485 window method to estimate the probability density function for each
 486 experiment. A normalization procedure was then adopted to increase
 487 the comparability between experiments. After normalization, the max-
 488 imum normalized activation weight was the same in each experiment.
 489 In this way, each experiment corresponding to a unique probability dis-
 490 tribution function was treated as independent. Even if many foci were
 491 reported in one experiment, it was also represented by a probability dis-
 492 tribution function, rather than treating the foci as independent.

493 Multiple comparison correction

494 As demonstrated in Eickhoff et al. (2012), an FDR correction was not
 495 appropriate for inferring the topological features (region of activations)
 496 from the statistical map derived from the ALE meta-analysis. So, an FWE

correction was adopted in CoPE. By randomly redistributing the coordi- 497
 nates in the experiments and performing the same analysis, the maxi- 498
 mum value of each permutation was preserved as an estimate of the 499
 distribution of the voxel-level peak values. The estimated distribution 500
 could then be used to define the FEW-corrected threshold. This estima- 501
 tion process had the advantage of not needing a pre-defined parameter- 502
 ization of the distribution, i.e., it was a non-parameter estimation. FWE 503
 correction has been exploited to provide a good estimate of the distribu- 504
 tion of the maximum cluster size in the MKDA method (Wager et al., 505
 2007). In the CoPE method, FWE correction was used to provide a 506
 voxel-level correction based on the distribution of the maximum co- 507
 activation weights from each permutation. However, if the maximum 508
 from each permutation was calculated precisely, the computational 509
 time would be rather great. Therefore, the Cauchy-Schwarz inequality 510
 was used to estimate a conservative upper bound for the maximum 511
 for each permutation to reduce the computing cost. In addition, the con- 512
 servative upper bound provided a more strict correction for the co- 513
 activation weight, which was beneficial for the power of the test. 514

Identification of the local convergence and long-range co-activation 515

In the CoPE method, the reported coordinates were used as the cen- 516
 ters of Gaussian distributions to model activation in the gray matter. 517
 Local convergence was reflected by the overlap between the estimated 518
 probability density functions. If the local convergence was high around a 519
 voxel, CoPE showed that the estimated probability density functions 520
 densely overlapped with each other across the experiments. Thus, al- 521
 though local convergence was primarily generated using the model, 522

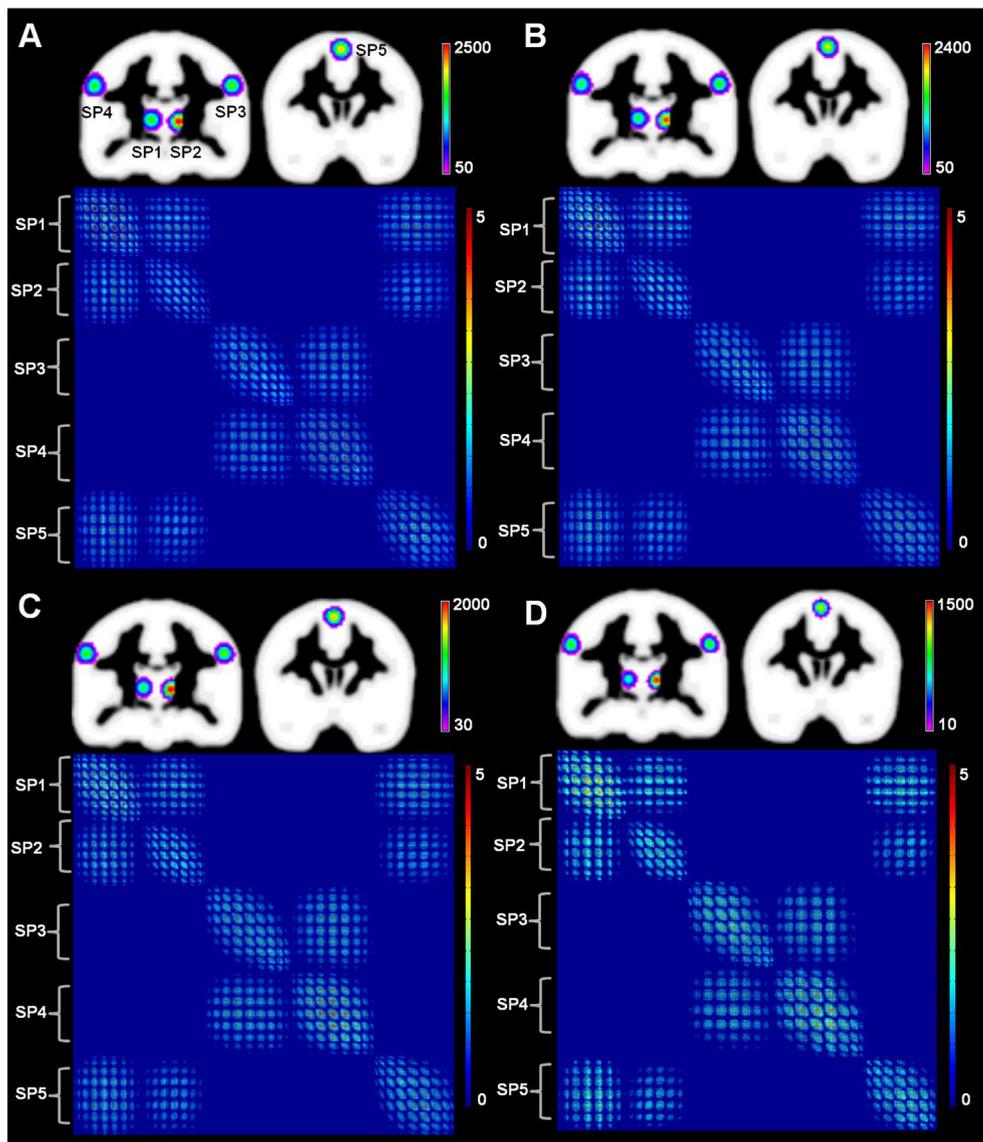


Fig. 6. Results of Simulation 5. The data was a simulation around five simulated points, i.e., from SP1 to SP5 (MNI: $-12\ 16\ 8$; $12\ -18\ 6$; $-56\ -16\ 36$; $56\ -16\ 36$; $0\ 6\ 60$). The noise increased from A to D. All of the results are the DDM derived using the CoPE method and the voxel-wise co-activation relationship corrected using an FWE at $p < 0.01$. (A) Without random noise. (B) The ratio of noise coordinates to information coordinates was 1:1. (C) The ratio of noise coordinates to information coordinates was 3:1. (D) The ratio of noise coordinates to information coordinates was 10:1.

local convergence could be considered as another way to represent consistent activation across a set of experiments. Long-range co-activations were particularly interesting, as they reflected the convergence of distant co-occurrences between two regions. Identifying long-range co-activations may contribute to mining the interactions between the brain architecture underlying specific cognitive domains. Networks of interactions between distant brain regions, including the default mode network and the salience network, have been identified from the whole BrainMap database using the ICA method (Ray et al., 2013; Smith et al., 2009). In addition, MACM has been used to model ROI-based co-activation patterns from the data in the BrainMap database (Eickhoff et al., 2011; Robinson et al., 2010). These methods indicate that long-range interactions can be identified in a coordinate-based database. Moreover, local and distant functional connectivity, which showed different distribution patterns in their brain regions, has been studied using resting-state and task fMRI data (Sepulcre et al., 2010). Sepulcre's study distinguished local from distant functional connectivity by whether they were within or beyond 14 mm (Sepulcre et al., 2010) and also found similar results using distances between 10 mm and 14 mm. In the CoPE method, this distance was decided using the

mean number of subjects across the experiments. Specifically, the CoPE method used 3 standard deviations (δ) from the mean number of subjects using the method in Eickhoff et al. (2009). When a reported peak was used as the center of a Gaussian distribution, the probability that a co-activated voxel was more than 3δ from the peak was negligible. In the working memory dataset, the distance for distinguishing long-range co-activation was set as 12.12 mm, which was 3δ from the mean, a number which was similar to the result in Sepulcre et al. (2010).

The simulation datasets

The analysis of the simulation datasets illustrated the capability of the CoPE method to find convergent activation regions, to infer voxel-wise local/long-range co-activations, and to resist random noise. Simulation 1 indicated that the local convergence could be detected by CoPE even in an extreme example (a single coordinate for an experiment with no co-activation between reported foci). This simulation illustrated that the brain regions possessing local convergence detected by CoPE were similar to that detected using the ALE method. Simulation 2 expanded the situation in Simulation 1 to show how CoPE would respond to simultaneous

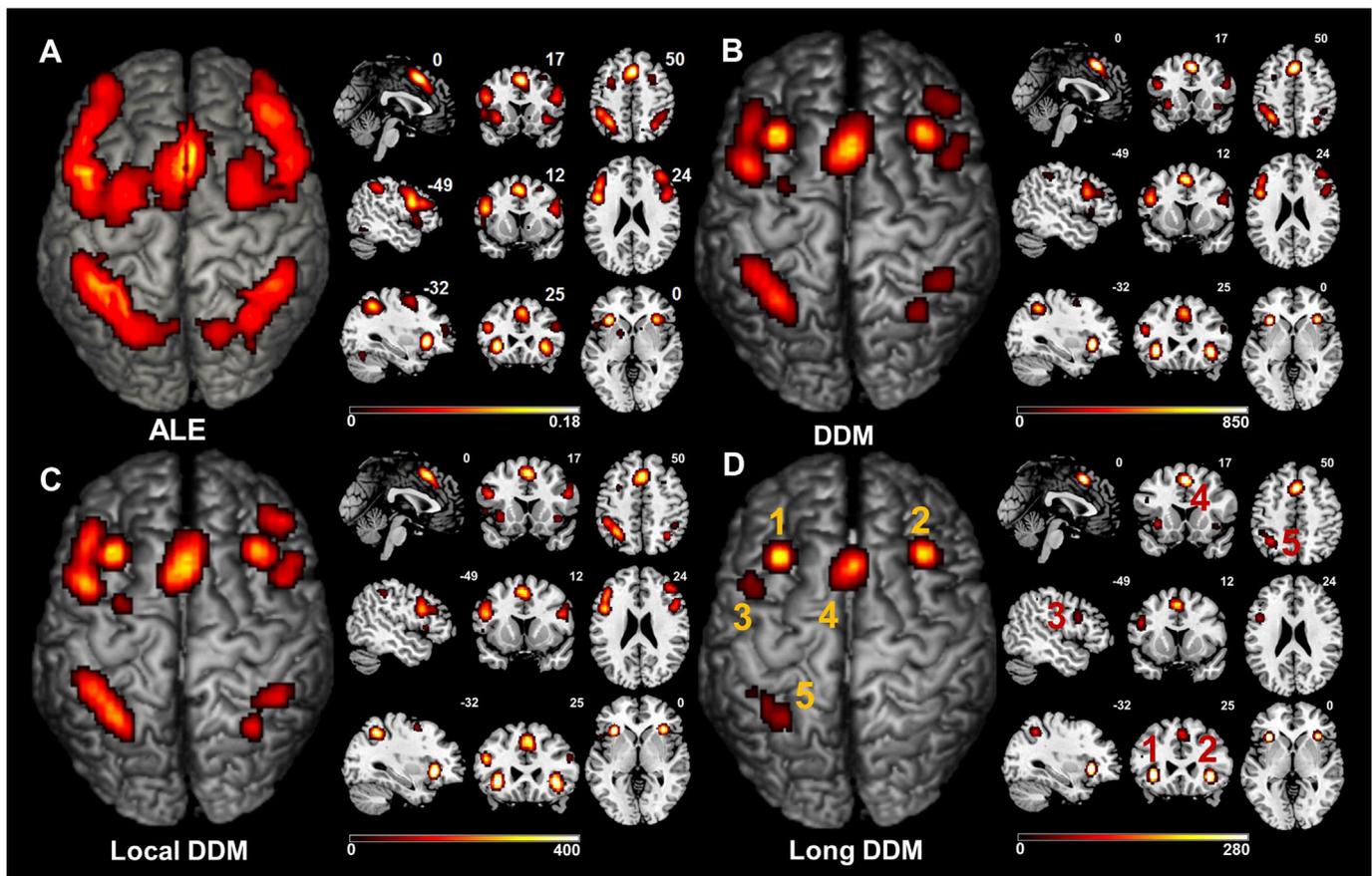


Fig. 7. The ALE and CoPE results from the working memory dataset. (A) The ALE results based on the working memory dataset. The threshold was $p < 0.05$ using a cluster-level FWE correction. (B) The degree density map (DDM) derived from the FWE-corrected voxel-wise co-activation matrix. The statistical significance of the co-activation was derived based on an FWE correction at $p < 0.05$. (C) The local DDM obtained using the CoPE method. The co-activations were separated into local and long-range based on a distance of 12.12 mm. (D) The long-range DDM (long DDM) obtained using the CoPE method. The numbers represent five clusters based on the criterion of whether a voxel was one of the 26 nearest neighbor voxels.

561 activation and co-activation. CoPE was still able to find the activation regions in Simulation 2 (Fig. 3A). Moreover, the voxel-wise co-activation was also derived (Fig. 3B). Further, Simulation 3 was supplementary to Simulation 2, but the activation and the co-activation were inconsistent, i.e., there was no co-activation between the two regions. When the

566 dataset of Simulation 3 was used, CoPE only found the activation regions (Fig. 4A), but the lack of co-activation became clear in the voxel-wise co-activation matrix (Fig. 4B). These simulations showed that CoPE was able to distinguish the activation and the co-activation relationships simultaneously. Simulation 4 demonstrated the effects of local convergence and

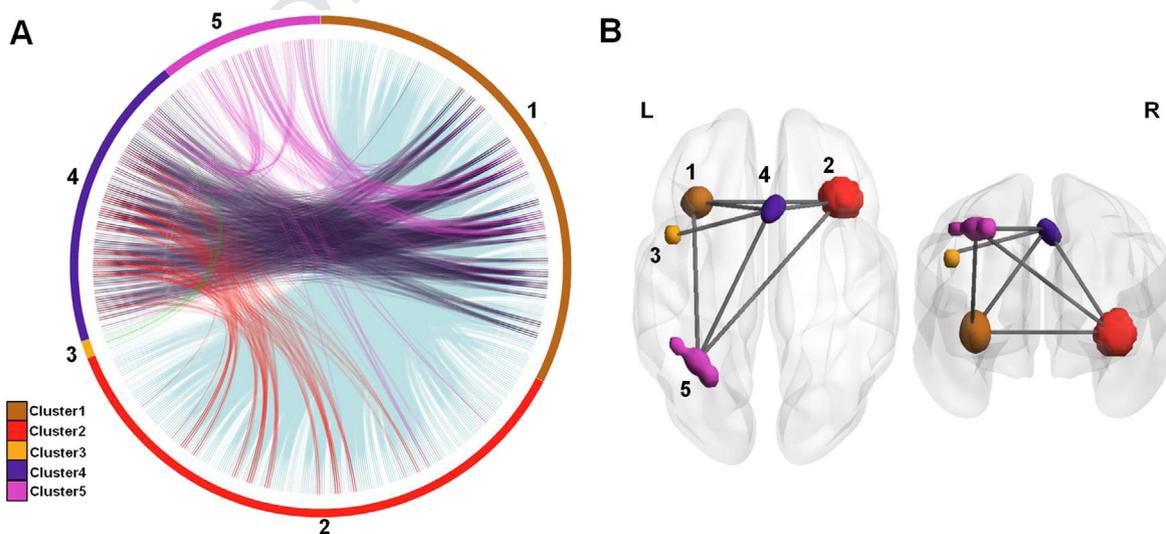


Fig. 8. The long-range co-activation relationships derived from the working memory dataset. (A) We identified 5 clusters derived from the long-range DDM using the criteria of whether a voxel was one of the 26 nearest neighbor voxels. The voxel-wise long-range co-activations were mapped between the clusters. (B) The clusters and the co-activation relationship projected in 3D space.

long-range co-activation. The difference between these provided the reason for distinguishing the activated regions based on the location of their co-activation. If the reported foci were activated independently, only local convergence occurred around the voxels. In Simulation 4, we could find not only the activation region (SP3), but also the co-activation regions (SP1 and SP2), using local/long-range co-activations (Fig. 5B and C). Moreover, the voxel-wise co-activations could be used to distinguish between the activation properties (local/long-range) of the regions (Fig. 5D). Simulation 5 showed that the CoPE method could be used to infer consistent results from heavy noise to light noise (Fig. 6). In fact, heavy noise resulted in a biased and weak activation compared with the noise-free condition, but the co-activation relationship was still similar among the different noise levels, and the densely co-activated regions had the same distribution pattern. To test whether the accuracy of CoPE would break down at very high noise levels, an extreme noise level was introduced. In the extreme high noise level, CoPE found only a little co-activation between SP3 and SP4 (Supplemental Fig. 2), but the local convergence was still preserved from SP1 to SP5. The ratio of the noise foci to informative foci was set at 300:3 in the experiments with reported foci around SP1, SP2, and SP5. The ratio of noise foci to informative foci was set at 200:2 in the experiments with reported foci around SP3 and SP4. The noise was severe in the experiments with reported foci around SP1, SP2 and SP5, so the co-activation was weaker around SP1, SP2 and SP5. Because CoPE was focused on co-activation relationship, random noise, which could not be consistently found to be co-activated with other signals, made little effect on the result. These simulations increased our confidence when we performed CoPE in a real application.

Working memory dataset

In the real dataset, the CoPE method was used not only to find the activation results that corresponded to the results obtained using ALE (Fig. 7A and B) but also to determine the long-range core task-dependent network (Figs. 7D and 8). The ALE method focused on convergent activations across experiments. The DDM (especially the long-range DDM) reflected the amount of (distant) co-activation of a voxel. On one hand, only voxels where activation occurs can have co-activations. On the other hand, not every activated region will necessarily have a significant degree of long-range co-activation. Because the dataset was from a previous study (Rottschy et al., 2012), the results from CoPE (DDM) largely reproduced the previous results in what can be considered to be a validation of the CoPE method. In other words, CoPE was able to identify the regions (those corresponding to the ones found by ALE; Fig. 7A and B) that would be reasonable to include in the network modeling in the next step. Because these processes reflect different aspects of the data, the DDM and the results from the ALE method were somewhat different (Fig. 7A and B). For example, the bilateral ventral visual cortex and lobule VI of the cerebellum, which were weakly activated in the ALE result, did not show up in the DDM.

Given the distance restriction, long-range co-activation that included the left BA 44, the SMA, left IPL, and bilateral insula was inferred (Fig. 7D). These brain regions were recognized as the 'core' network in the previous work (Rottschy et al., 2012). Moreover, the long-range co-activation network was lateralized to the left hemisphere, as was also found in the previous work using different task components (Rottschy et al., 2012). The deduced left-lateralization could be a clue for the functional distribution of working-memory. However, we cannot definitely conclude that the functional application of working-memory is left-lateralized because it may have just been a reflection of the co-activation of the data from the datasets in the reported studies. These studies may underrepresent the complete set of working memory research. For example, some researches indicated that the left prefrontal cortex was related to working memory retrieval (Oztekin et al., 2009), and the left hemisphere was found to be important in verbal working memory (Binder et al., 2009; D'Arcy et al., 2004; Nagel et al., 2013). But other studies of spatial working memory showed activations in

the right hemisphere (Jonides et al., 1993; Nagel et al., 2013; van Asselen et al., 2006).

Using the criterion of whether the voxels were among the 26 nearest neighbors, the voxel-wise co-activation was integrated into the between-cluster co-activation relationship between five clusters (Fig. 8). More precisely, clusters 1 and 2 were distributed at the junction between several brain regions, including the orbital IFG, triangular IFG, and anterior insula (Figs. 7D and 8B). This finding was in good agreement with a previous study in which foci in the IFG and anterior insula merged into a single cluster (Wager & Smith, 2003). This strong co-activation between clusters 1 and 2 indicates integration of the bilateral IFG and bilateral insula (Fig. 8B). Engagement of the insula in working memory encoding, maintenance, and retrieval has been noted in previous studies (Mohr et al., 2006; Munk et al., 2002; Pessoa et al., 2002). The fronto-parietal network, which is the widespread brain functional location of the working memory during working memory performance, was partially revealed in our result. We found strong long-range co-activation between the left IPL and the SMA (cluster 5 and cluster 4; Fig. 8B) and co-activation between the left IPL and the insula (cluster 5, cluster 1 and cluster 2; Fig. 8B). The prefrontal cortex (PFC) was not revealed as a single cluster that possessed strong co-activation with the parietal cortex (PC). However, clusters 1 and 2 included partial regions of the IFG. So, the co-activations between cluster 5, cluster 2, and cluster 1 may have represented an integrated result from the IFG, insula, and left IPL. The engagement of the SMA in working memory has been observed as a major effect in previous meta-analyses (Owen et al., 2005; Rottschy et al., 2012; Wager & Smith, 2003). In addition, the co-activation pattern corresponded with a previous fMRI study which found significant functional connectivity between the left Sylvian-parietal-temporal area (Spt) and regions located at the junction of the anterior insula and the IFG and significant functional connectivity between left Spt and the pre-SMA during the memory-encoding stage (Hashimoto et al., 2010). Moreover, there was co-activation between the left opercular IFG (located in BA 44) and the SMA, i.e., cluster 3 and cluster 4. The engagement of the SMA and BA 44 in working memory tasks has been observed in several studies (Barber et al., 2013; Chein & Fiez, 2001). Noting that cluster 3 was significantly co-activated only with cluster 4, it is possible that cluster 3 participated in the working memory task through cluster 4.

The significant co-activation relationships mined from the data should be considered as clues to probable functional relationships. In fact, following the definition of functional connectivity as the temporal coincidence of spatially remote neurophysiological events (Friston, 1994), co-activation might be regarded as functional connectivity in which the (temporal) unit of observation was the experiment. Validation of the relationship between the mined co-activation and brain function needs further studies, including some that adopt new samples or new paradigms.

Conclusion

In this study, we proposed a new method named CoPE to mine a voxel-wise task-dependent co-activation network based on foci reported in a number of experiments. In CoPE, the Parzen window method was performed to model the activation within an experiment. The weight of the co-activation was defined as the product of the individual normalized probabilities of the activations summed across the experiments. For the significance test, to save on the high computational costs of calculating the permutations, CoPE used a conservative FWE for multiple comparisons. Simulation data demonstrated that CoPE could not only find convergent activation brain regions but also be used to infer the voxel-wise co-activation pattern. CoPE also generated stable results in both low and high noise levels. Furthermore, CoPE found a left-lateralized network in a working memory dataset. The long-range co-activation was of particular interest in that it may reflect the co-activation between distant regions. From these results, it seems

that mining voxel-wise co-activations from previous studies could provide clues about what to look for and how to perform future studies.

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Appendix A. Supplementary data

Supplementary data to this article can be found online at <http://dx.doi.org/10.1016/j.neuroimage.2015.05.069>.

References

- Barber, A.D., Caffo, B.S., Pekar, J.J., Mostofsky, S.H., 2013. Effects of working memory demand on neural mechanisms of motor response selection and control. *J. Cogn. Neurosci.* 25, 1235–1248.
- Binder, J.R., Desai, R.H., Graves, W.W., Conant, L.L., 2009. Where is the semantic system? A critical review and meta-analysis of 120 functional neuroimaging studies. *Cereb. Cortex* 19, 2767–2796.
- Chein, J.M., Fiez, J.A., 2001. Dissociation of verbal working memory system components using a delayed serial recall task. *Cereb. Cortex* 11, 1003–1014.
- D'Arcy, R.C., Ryner, L., Richter, W., Service, E., Connolly, J.F., 2004. The fan effect in fMRI: left hemisphere specialization in verbal working memory. *Neuroreport* 15, 1851–1855.
- Eickhoff, S.B., Laird, A.R., Grefkes, C., Wang, L.E., Zilles, K., Fox, P.T., 2009. Coordinate-based activation likelihood estimation meta-analysis of neuroimaging data: a random-effects approach based on empirical estimates of spatial uncertainty. *Hum. Brain Mapp.* 30, 2907–2926.
- Eickhoff, S.B., Jbabdi, S., Caspers, S., Laird, A.R., Fox, P.T., Zilles, K., Behrens, T.E.J., 2010. Anatomical and functional connectivity of cytoarchitectonic areas within the human parietal operculum. *J. Neurosci.* 30, 6409–6421.
- Eickhoff, S.B., Bzdok, D., Laird, A.R., Roski, C., Caspers, S., Zilles, K., Fox, P.T., 2011. Co-activation patterns distinguish cortical modules, their connectivity and functional differentiation. *Neuroimage* 57, 938–949.
- Eickhoff, S.B., Bzdok, D., Laird, A.R., Kurth, F., Fox, P.T., 2012. Activation likelihood estimation meta-analysis revisited. *Neuroimage* 59, 2349–2361.
- Evans, A.C., Marrett, S., Neelin, P., Collins, L., Worsley, K., Dai, W., Milot, S., Meyer, E., Bub, D., 1992. Anatomical mapping of functional activation in stereotaxic coordinate space. *Neuroimage* 1, 43–53.
- Evans, A.C., Kamber, M., Collins, D.L., Macdonald, D., 1994. An MRI-based probabilistic atlas of neuroanatomy. *Magn. Reson. Scan. Epilepsy* 264, 263–274.
- Fox, P.T., Friston, K.J., 2012. Distributed processing; distributed functions? *Neuroimage* 61, 407–426.
- Fox, P.T., Lancaster, J.L., 2002. Opinion: mapping context and content: the BrainMap working model. *Nat. Rev. Neurosci.* 3, 319–321.
- Friston, K.J., 1994. Functional and effective connectivity in neuroimaging: a synthesis. *Hum. Brain Mapp.* 2, 56–78.
- Hashimoto, R., Lee, K., Preus, A., McCarley, R.W., Wible, C.G., 2010. An fMRI study of functional abnormalities in the verbal working memory system and the relationship to clinical symptoms in chronic schizophrenia. *Cereb. Cortex* 20, 46–60.
- Jonides, J., Smith, E.E., Koeppe, R.A., Awh, E., Minoshima, S., Mintun, M.A., 1993. Spatial working memory in humans as revealed by PET. *Nature* 363, 623–625.
- Kadison, R.V., 1952. A generalized Schwarz inequality and algebraic invariants for operator algebras. *Ann. Math.* 56, 494–503.
- Laird, A.R., Lancaster, J.L., Fox, P.T., 2005. BrainMap: the social evolution of a human brain mapping database. *Neuroinformatics* 3, 65–78.

- Laird, A.R., Eickhoff, S.B., Li, K., Robin, D.A., Glahn, D.C., Fox, P.T., 2009. Investigating the functional heterogeneity of the default mode network using coordinate-based meta-analytic modeling. *J. Neurosci.* 29, 14496–14505.
- Laird, A.R., Eickhoff, S.B., Rottschy, C., Bzdok, D., Ray, K.L., Fox, P.T., 2013. Networks of task co-activations. *Neuroimage* 80, 505–514.
- Lancaster, J.L., Tordesillas-Gutierrez, D., Martinez, M., Salinas, F., Evans, A., Zille, S., K., Mazziotta, J.C., Fox, P.T., 2007. Bias between MNI and Talairach coordinates analyzed using the ICBM-152 brain template. *Hum. Brain Mapp.* 28, 1194–1205.
- Mohr, H.M., Goebel, R., Linden, D.E., 2006. Content- and task-specific dissociations of frontal activity during maintenance and manipulation in visual working memory. *J. Neurosci.* 26, 4465–4471.
- Munk, M.H., Linden, D.E., Muckli, L., Lanfermann, H., Zanella, F.E., Singer, W., Goebel, R., 2002. Distributed cortical systems in visual short-term memory revealed by event-related functional magnetic resonance imaging. *Cereb. Cortex* 12, 866–876.
- Nagel, B.J., Herting, M.M., Maxwell, E.C., Bruno, R., Fair, D., 2013. Hemispheric lateralization of verbal and spatial working memory during adolescence. *Brain Cogn.* 82, 58–68.
- Nichols, T., Hayasaka, S., 2003. Controlling the familywise error rate in functional neuroimaging: a comparative review. *Stat. Methods Med. Res.* 12, 419–446.
- Owen, A.M., McMillan, K.M., Laird, A.R., Bullmore, E., 2005. N-back working memory paradigm: a meta-analysis of normative functional neuroimaging studies. *Hum. Brain Mapp.* 25, 46–59.
- Oztekin, I., McElree, B., Staresina, B.P., Davachi, L., 2009. Working memory retrieval: contributions of the left prefrontal cortex, the left posterior parietal cortex, and the hippocampus. *J. Cogn. Neurosci.* 21, 581–593.
- Parzen, E., 1962. Estimation of a probability density-function and mode. *Ann. Math. Stat.* 33, 1065.
- Pessoa, L., Gutierrez, E., Bandettini, P., Ungerleider, L., 2002. Neural correlates of visual working memory: fMRI amplitude predicts task performance. *Neuron* 35, 975–987.
- Poldrack, R.A., Mumford, J.A., Schonberg, T., Kalar, D., Barman, B., Yarkoni, T., 2012. Discovering relations between mind, brain, and mental disorders using topic mapping. *Plos Comput. Biol.* 8.
- Ray, K.L., McKay, D.R., Fox, P.M., Riedel, M.C., Uecker, A.M., Beckmann, C.F., Smith, S.M., Fox, P.T., Laird, A.R., 2013. ICA model order selection of task co-activation networks. *Front. Neurosci.* 7, 237.
- Robinson, J.L., Laird, A.R., Glahn, D.C., Lovallo, W.R., Fox, P.T., 2010. Metaanalytic connectivity modeling: delineating the functional connectivity of the human amygdala. *Hum. Brain Mapp.* 31, 173–184.
- Rosenblatt, M., 1956. Remarks on some nonparametric estimates of a density-function. *Ann. Math. Stat.* 27, 832–837.
- Rottschy, C., Langner, R., Dogan, I., Reetz, K., Laird, A.R., Schulz, J.B., Fox, P.T., Eickhoff, S.B., 2012. Modelling neural correlates of working memory: a coordinate-based meta-analysis. *Neuroimage* 60, 830–846.
- Sepulcre, J., Liu, H.S., Talukdar, T., Martincorena, I., Yeo, B.T.T., Buckner, R.L., 2010. The organization of local and distant functional connectivity in the human brain. *Plos Comput. Biol.* 6.
- Smith, S.M., Fox, P.T., Miller, K.L., Glahn, D.C., Fox, P.M., Mackay, C.E., Filippini, N., Watkins, K.E., Toro, R., Laird, A.R., Beckmann, C.F., 2009. Correspondence of the brain's functional architecture during activation and rest. *Proc. Natl. Acad. Sci. U. S. A.* 106, 13040–13045.
- Steele, J.M., 2004. The Cauchy–Schwarz Master Class : An Introduction to the Art of Mathematical Inequalities. Cambridge University Press, Cambridge; New York.
- Talairach, J., Tournoux, P., 1988. Co-planar Stereotaxic Atlas of the Human Brain: 3-Dimensional Proportional System: An Approach to Cerebral Imaging. Georg Thieme, Stuttgart, New York.
- Toro, R., Fox, P.T., Paus, T., 2008. Functional coactivation map of the human brain. *Cereb. Cortex* 18, 2553–2559.
- Turkeltaub, P.E., Eden, G.F., Jones, K.M., Zeffiro, T.A., 2002. Meta-analysis of the functional neuroanatomy of single-word reading: method and validation. *Neuroimage* 16, 765–780.
- Turkeltaub, P.E., Eickhoff, S.B., Laird, A.R., Fox, M., Wiener, M., Fox, P., 2012. Minimizing within-experiment and within-group effects in activation likelihood estimation meta-analyses. *Hum. Brain Mapp.* 33, 1–13.
- van Asselen, M., Kessels, R.P., Neggers, S.F., Kappelle, L.J., Frijns, C.J., Postma, A., 2006. Brain areas involved in spatial working memory. *Neuropsychologia* 44, 1185–1194.
- Wager, T.D., Smith, E.E., 2003. Neuroimaging studies of working memory: a meta-analysis. *Cogn. Affect. Behav. Neurosci.* 3, 255–274.
- Wager, T.D., Jonides, J., Reading, S., 2004. Neuroimaging studies of shifting attention: a meta-analysis. *Neuroimage* 22, 1679–1693.
- Wager, T.D., Lindquist, M., Kaplan, L., 2007. Meta-analysis of functional neuroimaging data: current and future directions. *Soc. Cogn. Affect. Neurosci.* 2, 150–158.
- Yarkoni, T., Poldrack, R.A., Nichols, T.E., Van Essen, D.C., Wager, T.D., 2011. Large-scale automated synthesis of human functional neuroimaging data. *Nat. Methods* 8, 665–670.